

503

Synergies: Stabilities, instabilities, and modes

E. Saltzman^a and J. A. S. Kelso^{a,b}

^aHaskins Laboratories, New Haven, Conn. 06511 and ^bDepartment of Psychology and Biobehavioral Science, University of Connecticut, Storrs, Conn. 06268

Nashner & McCollum (N & M) have addressed the question of whether muscle synergies exist for complex skilled activity, and if so, how they are organized (see also Kelso & Tuller 1983/1984; Lee 1984). The authors argue that muscle synergies exist for

postural stability tasks in the form of a small set of discretely represented control entities, and that postural corrective movements of the dynamically continuous musculoskeletal system are organized through the operation of these discrete synergy elements. In this commentary, we make two main points: first, that N & M's arguments are not supported sufficiently by their data (i.e., the data do not allow one to distinguish between their discrete synergy model and other model types); we will describe the sort of data that would be convincing. And second, because N & M stress the "universality and importance of global schemes" for sensorimotor coordination and "principles governing the interactions among elements" that lead to "testable hypotheses," we mention briefly a theoretical framework that is attractive to us (e.g., Kelso 1984; Kelso & Saltzman 1982; Kelso & Tuller 1983/1984; Kugler, Kelso & Turvey 1980, 1982) because it treats cooperative phenomena in multicomponent systems on the basis of first principles (e.g., Haken 1975). We feel that this framework can: (1) offer a firmer basis for some of N & M's existing experimental observations; and (2) promote an experimental strategy that would illuminate N & M's hypothesis of region-specific discrete synergies.

N & M describe distinct patterns of EMG (electromyogram) bursts in response to distinct patterns of postural perturbation (e.g., vertical or front-back platform translation) in the context of given support conditions (e.g., different platform sizes). Each EMG pattern is characterized by a temporally ordered sequence of bursts within a subset of three agonist-antagonist muscle pairs (ankle, thigh, and trunk muscles). N & M hypothesize that each such pattern or synergy operates with respect to a corresponding distinct control structure. Each structure controls corrective postural movements within a limited subregion of postural configuration space (e.g., ankle angle versus hip angle plane), such that when the body is perturbed the associated (fine-tuned) EMG burst pattern will return the body to a balanced posture. In principle, however, such synergistic EMG patterns could also be generated by alternative models (e.g., Litvintsev 1972; Saltzman & Kelso 1984) in which control laws dependent on task (i.e., maintain balance), support condition, and postural configuration serve continually to specify corrective joint torque vectors that return the body from an unbalanced to a balanced posture. If one defined a further mapping from torque vectors to "muscle element" vectors (e.g., Jerard & Jacobsen 1980; Saltzman 1979) for which muscle elements were activated only after inputs exceeded a given threshold, then ongoing corrective torques would be mapped into patterns of discrete EMG bursts in those muscles appropriate for producing the required torques. This sort of control-law model augmented by thresholds for muscle element recruitment should generate consistent "synergistic" patterns of postural EMG in response to given types of destabilizing inputs, without reference to discretely organized synergy control structures. For stabilizing movements initiated from most locations in the postural configuration space, therefore, the above discrete and control-law hypotheses predict qualitatively similar EMG activity patterns. However, the discrete synergy model predicts that there will be certain regions of the configuration space for which the EMG predictions will be different for discrete and control-law models.

For the discrete control hypothesis, partitioning the configuration space into distinct (possibly overlapping) synergy subregions implies that border-lines (or border regions) will be defined between the different control domains (see N & M's Figure 5). N & M's notion implies that the system will behave differently along (or within) these borders than when operating away from them. Furthermore, when the postural system adapts from one support condition to another (e.g., from long to short platform lengths) the implication is that the border layout itself shifts correspondingly. Let us focus on the "simpler" adapted case for which border structure is assumed to be relatively constant. In this instance, the control structures

associated with adjacent configurational domains should compete equally at the borders for access to the final common path of muscular output. There are at least four possible outcomes of such competition: (a) opposing effects will cancel each other and no muscle activity will occur; (b) competing synergies will be observed simultaneously in a mixture of EMG patterns; (c) there will be a repetitive alternation or "jittering" between the EMG patterns of each competing synergy; or (d) a totally novel EMG pattern might be observed. Experimental demonstration of any of these patterns near N & M's hypothesized synergy borders in support-condition-adapted subjects would provide strong support for the discrete model, since the control-law model would not behave differently on, near, or away from those borders. These data are lacking, however, or at least have not been presented in the target article. The strongest data offered by N & M in favor of their hypothesis is the sequential mixing of ankle and hip "synergies" during adaptation to suddenly change platform sizes (see N & M's Figure 7). However, these findings seem equivocal at best, given the concomitant shifts in border structure that presumably accompany such adaptation. Therefore, perturbation studies that use adapted subjects and that explore a sufficiently large sample of the postural space could: (1) help to identify synergy borders and (2) constitute a direct test of the discrete synergy model.

The above suggestion exemplifies a general experimental strategy for explicating the cooperative behavior of multicomponent, open, nonlinear systems. A common feature of all such systems is that when control parameters are changed beyond certain critical values, new "modes" or spatiotemporal patterns may appear (for many examples in physics, chemistry, and biology see Haken 1977, 1983; Prigogine 1980; Yates 1982; Yablonsky & Iberall 1973; for examples in motor behavior, see Colquhoun, Holmes, & Rand 1982; Kelso & Tuller 1983/1984; von Holst 1973). The beauty of this formulation is that the modes (i.e., synergistic patterns) may themselves be described by a set of dynamical equations derived via transformation procedures from the equations describing the behavior of the original subsystems (e.g., muscle elements). Under the influence of a continuous parameter scaling a given mode may suddenly become dominant and "capture" the behavior of the subsystem. Such bifurcations result from the competition, as it were, between the "forces" or inputs that are parametrically scaled (corresponding, for example, to the translation of a platform) and the "forces" holding the system together (i.e., the synergistic constraints among muscles).

In Figure 1 we show an example from our own work on cooperative behavior in a parametrically scaled, bimanual movement system exhibiting such a bifurcation. In the figure, the displacement time profiles of left and right hands are plotted against each other on the Lissajous plane. Here the phase relation between the movements of the right and left hands describes the spatiotemporal ordering among corresponding flexor and extensor muscle activities. Starting in the antiphase modal pattern (right flexion [extension] is accompanied by left extension [flexion]), the parameter of movement frequency is varied and increased in a continuous manner. As the frequency increases the antiphase mode becomes less stable, as exemplified by an increase in phase variance. At a critical value (which turns out to be a dimensionless function of each individual's preferred cycling rate), the system bifurcates and a different, in-phase modal pattern appears (for a more complete analysis, see Kelso 1984). Extrapolating the above concepts to the postural domain of N & M, we envisage one "discrete strategy" as giving way to another at critical borders in the postural parameter space.

Several points, therefore, are pertinent to N & M's analysis. First, transitions from one synergistic pattern of muscle elements to another may be discontinuous, even though the process controlling the process can change continuously. Second, discontinuities of muscular pattern (giving rise to a description with apparently discrete properties) are observed not because

SELF GENERATED PHASE TRANSITION

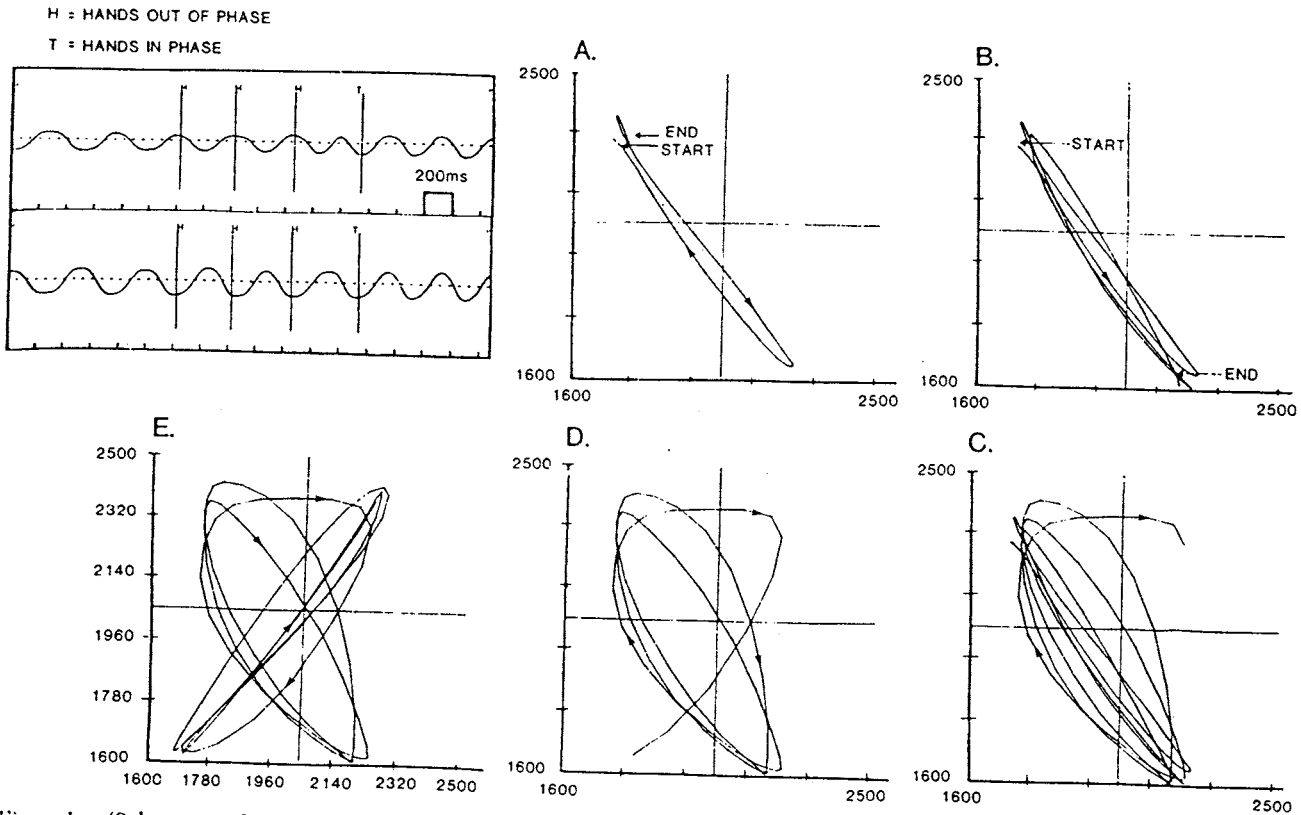


Figure 1. (Saltzman and Kelso) Angular position-time profiles of left and right hands (upper left) and position of each plotted against the other on the Lissajous plane (A-E). Left and right hand positions are plotted on the X and y axes respectively. "Hands out of phase" means that flexion of one hand is accompanied by extension of the other and vice versa. "Hands in phase" means that both hands flex and extend at about the same time. Phase becomes less stable (1C) as evident in the widening of the Lissajous trajectory, until an abrupt transition occurs (1D) (from Kelso & Tuller 1983/1984).

are no intervening behavioral states, but because none of them is stable (see possible experimental outcomes above). Thus, there may be a large number of ways for a system to exhibit continuous change but only a small number of ways for it to change discontinuously. To conclude, therefore, that discrete logical control is *imposed* upon a continuous mechanical system may not be warranted. Rather, synergistic muscular activities may *emerge* as modal patterns from appropriately scaled neuromuscular dynamical systems. Finally, although discrete logical states could be used to represent distinct modal patterns, it should be recognized that much of this apparent discreteness reflects the larger time constants of the dominant modes relative to the time constants of the subsystems. With reference to postural control, synergistic patterning among muscles appropriate to a given region of the associated parameter space is defined over longer time spans than, say, those involved in motor unit recruitment. Thus, the discrete-logical versus continuous-dynamical distinction drawn by Nashner & McCollum may be more apparent than real.

ACKNOWLEDGMENTS

Preparation of this paper and some of the research discussed therein were supported by ONR Grant N00014-S3-0083 and NIH Grant NS-13617.